

Effects of Growth Factors in Vivo

I. Cell Ingrowth Into Porous Subcutaneous Chambers

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Growth factors secreted by platelets and macrophages may play roles in atherogenesis and in wound repair. The multiple biologic effects of these factors are being studied extensively *in vitro*, but their roles *in vivo* are relatively unexplored. The cellular responses to platelet-derived growth factor (PDGF), transforming growth factor beta (TGF β), basic fibroblast growth factor (bFGF), and epidermal growth factor (EGF) were examined in a wound chamber model in rats. Growth factors were emulsified in bovine dermal collagen suspensions, placed in 1 \times 30-mm porous polytetrafluoroethylene tubes, inserted subcutaneously, and removed after 10 days. The presence of PDGF (400 ng), TGF β (200 ng), or bFGF (100 ng) increased the DNA content of the chambers two- to sixfold, compared with controls. Regardless of dose, EGF (100–800 ng) did not affect the DNA content. The increases in DNA observed for PDGF, TGF β , or bFGF resulted from accumulations of varying numbers of fibroblasts, capillaries, macrophages, and leukocytes in 10-day chambers. The addition of 250 μ g/ml heparin to the

collagen suspension potentiated the response to PDGF and bFGF, but not to TGF β or EGF. The clearance of ¹²⁵I-labeled growth factors from the chambers was biphasic. After an initial rapid phase, the remaining growth factor was slowly cleared. The half-life of the initial phase was rapid for PDGF (12 hours) and bFGF (9 hours) and somewhat slower for TGF β (22 hours). There was no difference in the rate of clearance between collagen and collagen/heparin matrices for any of the growth factors examined. These studies demonstrate that PDGF, bFGF, and TGF β can induce granulation tissue development in normal animals. The similarity in cellular responses to three peptides with differing *in vitro* actions suggests that the responses observed at 10 days reflect a secondary process, possibly mediated by effector cells such as macrophages, lymphocytes, or granulocytes that are attracted into the chamber by each growth factor, rather than a direct effect of the factors themselves. (Am J Pathol 1987, 129:601–613)

GROWTH FACTORS secreted by platelets and activated macrophages have been postulated to play numerous roles in repair of tissue injury and development of vascular diseases. *In vitro*, these growth factors can stimulate cell proliferation, cell migration, and changes in extracellular matrix composition of specific target cells.^{1–4} Each of these actions could be important in the process of healing wounds or in the development of proliferative vascular lesions. Whether any or all of these growth factors are deposited and act *in vivo* is not yet known. The objective of these experiments was to observe the effects of platelet-derived growth factor (PDGF), basic fibroblast growth factor (bFGF), type beta transforming growth factor (TGF β), and epidermal growth factor (EGF) in the complex milieu of the intact animal.

The growth factors examined are all contained in platelets, activated monocytes, or macrophages, cell types that appear to play important roles in wound healing^{5,6} and atherosclerosis.⁷ Although some of the biologic activities of these factors overlap, each has a unique combination of activities and target cells that are affected. PDGF is released from platelets,⁸ monocytes,⁹ and macrophages^{10,11} and is capable of stimu-

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lating mesenchymal cell migration and proliferation (reviewed by Ross et al¹). The basic form of FGF has been demonstrated in serum¹² and in lysates of mouse peritoneal exudate cells.¹³ Basic FGF is an endothelial cell mitogen¹⁴ and also stimulates the proliferation of fibroblasts *in vitro* (reviewed by Gospodarowicz³). The third growth factor examined, TGF β , is present in platelets¹⁵⁻¹⁷ and can be formed and released by monocytes and macrophages.¹⁸ In cell culture, TGF β tends to inhibit monolayer fibroblast proliferation and under specific conditions can stimulate cell growth in soft agar.^{19,20} It is a potent chemoattractant for monocytes²¹ and fibroblasts²² and, when injected subcutaneously in neonatal mice, can result in fibroplasia.²³ Epidermal growth factor (EGF) is present in platelets²⁴ and may be formed by activated macrophages as well.²⁵ EGF stimulates epithelial cells to migrate²⁶ and proliferate⁴ and can also stimulate fibroblast proliferation.²⁷

We have studied the accumulation of cells in porous expanded polytetrafluoroethylene chambers implanted subcutaneously in rats. Chambers were filled with an emulsification of bovine collagen and one or more of the growth factors. We find that some, but not all, of these growth factors stimulate a cellular response in the lumen of the chambers and that addition of heparin to the collagen matrix enhances the responses to PDGF and bFGF.

Materials and Methods

Animals

Male Sprague-Dawley rats weighing 350–400 g were obtained from Tyler Laboratories, Bellevue, Washington. The animals were housed in the Division of Animal Medicine facility at the University of Washington. Food and water were available *ad libitum*, and a 12-hour light/dark schedule was maintained. Rats were anesthetized for all surgical procedures by sequential injections of 40 mg pentobarbital/kg intraperitoneally (Anthony Products Company, Arcadia, Calif) and 0.1 ml Innovar-Vet/kg intramuscularly (fentanyl/droperidol, Pittman-Moore, Inc., Washington Crossing, NJ).

Growth Factors

PDGF was prepared from outdated human platelets as previously described.²⁸ For some experiments, a partially purified PDGF preparation was used. This preparation was a pool of the side fractions collected from S200 and heparin-Sepharose columns during PDGF purification. All mitogenic activity of the crude material could be inhibited by preincubation

with a polyclonal goat anti-PDGF IgG. PDGF was used at a dose of 8 μ g/ml collagen suspension (approximately 400 ng/chamber). TGF β was the generous gift of Drs. Michael Sporn and Anita Roberts, National Cancer Institute, Bethesda, Maryland. The TGF β used was isolated from outdated human platelets.¹⁶ TGF β was used at a dose of 4 μ g/ml collagen suspension (approximately 200 ng/chamber). The basic form of fibroblast growth factor was prepared and kindly provided by Dr. Andrew Baird of the Salk Institute for Biological Studies, La Jolla, California. Basic FGF (bFGF) was isolated from bovine pituitary.¹⁴ The dose of bFGF used routinely was 2 μ g/ml collagen suspension (approximately 100 ng/chamber). Receptor grade EGF, isolated from mouse submaxillary glands, was purchased from Collaborative Research, Inc., Waltham, Massachusetts. EGF was tested at doses from 2–16 μ g/ml collagen suspension (approximately 100–800 ng/chamber). The basic collagen matrix used in these experiments was pepsin-solubilized, reconstituted bovine dermal collagen dispersed in saline.²⁹ Final protein concentration in the chambers was 25–27 mg collagen/ml. Previous characterization of this collagen preparation showed it to be composed of greater than 95% Type I collagen, with the remainder being Type III.²⁹ Fibrillar collagen/heparin composites were also utilized for growth factor delivery in these experiments. Preparation and characterization of these formulations has been previously described.³⁰ Collagen/heparin 1 (CH1) included 300 μ g heparin/ml stock collagen suspension (250 μ g heparin/ml collagen emulsification in chambers). The source of the heparin was Hepar Industries, Franklin, Ohio. The formulation designated collagen/heparin 2 (CH2) consisted of collagen emulsion premixed with heparin but in a lower concentration (50 μ g heparin/ml stock collagen suspension, 41.5 μ g heparin/ml collagen emulsification in chambers). All collagen preparations were prepared and provided by Collagen Corporation, Palo Alto, California.

Preparation of Wound Chambers

Each chamber consisted of a 1 \times 30-mm tube of expanded polyfluorotetraethylene (PTFE) with a nominal pore size of 90 μ (GORE-TEX Expanded PTFE Cell Collector Tubing, generously supplied by W. L. Gore & Associates, Inc., Flagstaff, Ariz). The chambers were filled with an emulsification of growth factors and collagen or collagen/heparin under sterile conditions, and both ends of each chamber were tied with silk suture. Each chamber contained approximately 50 μ l of the collagen growth factor mixture.

With a 13-gauge needle as a trocar, four to six chambers were inserted under the abdominal skin of anesthetized rats (Figure 1). In a given rat, all chambers had the same matrix: collagen, CH1, or CH2. The chambers were removed at various times after insertion and cut into four 5-mm segments. Two alternating segments were taken for DNA assay, and the remaining two segments were fixed in methanol-Carnoy's solution for histologic evaluation.

Analysis for DNA Content and Histology

After digestion for 48 hours in 1 M NaOH, duplicate aliquots were precipitated with trichloroacetic acid and extracted with potassium acetate in ethanol, then incubated with diaminobenzoic acid and the DNA content determined fluorimetrically.³¹ Methanol-Carnoy's-fixed segments were embedded in paraffin, and 5- μ sections were cut and stained with hematoxylin and eosin (H&E) for histologic evaluation.

Clearance Studies

To determine how long the growth factors were retained in the collagen-filled chambers, a separate set of experiments was performed. Trace concentrations (0.1 μ g/ml) of ¹²⁵I-growth factor were added to the growth factor solutions prior to emulsification with collagen, CH1, or CH2. Six chambers were filled with each emulsification, and all six chambers were inserted in the same rat. The chambers were removed under ether anesthesia 1, 10, 24, 48, 120, and 240 hours after insertion. The amount of ¹²⁵I-growth factor in each chamber was quantified before insertion

and after removal by counting the chambers in a Beckman Gamma 4000 counter. Results are expressed as "percent counts remaining," comparing the counts in each chamber after removal with its preinsertion counts. Initial counts in individual chambers ranged from 300,000 to 700,000 cpm, depending upon the growth factor used.

Statistics

Comparisons of the effects of collagen versus collagen/heparin as a matrix for each treatment were made with the Mann-Whitney U test ($P < 0.05$). Treatment effects within the collagen or collagen/heparin groups were assessed using the Kruskal-Wallis one-way ANOVA for ranks. Specific comparisons between treatments were tested by Dunn's procedure (experimentwise, $P < 0.1$).

Results

Wound Chamber Model

After implantation in normal rats, the cellular response in subcutaneous porous chambers containing a collagen matrix or purified growth factors emulsified in the collagen matrix were evaluated for DNA content and histology at 10 days. Preliminary experiments (data not shown) were performed to establish which doses of growth factors to study in more detail and which time point to evaluate. A dose of each growth factor that resulted in a reproducible response (assessed by DNA content and histology) was selected for further study. Ten days was chosen as the end point because fibroplasia and neovascularization in response to PDGF and TGF β were well established by 10 days but still variable at 8 days. The responses did not increase significantly if the chambers were left in the animals for 22 days.

As a control, phosphate-buffered saline containing 0.25% BSA (vehicle) was emulsified with the appropriate collagen matrix, and one chamber containing this emulsion was inserted in each rat for monitoring basal responses. Ten days after insertion, very few cells were seen in the collagen-filled lumen of vehicle-treated chambers with either the collagen or CH1 matrix (Figure 2A and B). Some cells were present in the interstices of the PTFE. The DNA content of such chambers was typically low and not affected by the addition of heparin to the matrix (Figure 3). The PTFE elicited a mild foreign-body reaction, reflected in the presence of leukocytes and giant cells at the outside margin of the PTFE. The number of these inflammatory cells was similar in all treatments, vehicle or growth factor.

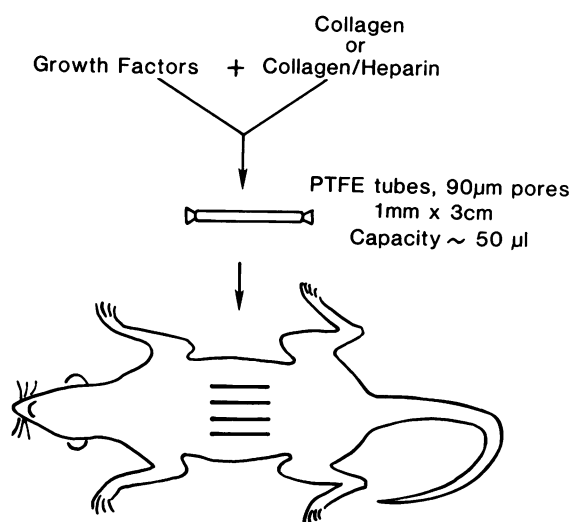


Figure 1—Schematic diagram of subcutaneous chamber model. Typically, four chambers were inserted under the abdominal skin of each rat, as shown.

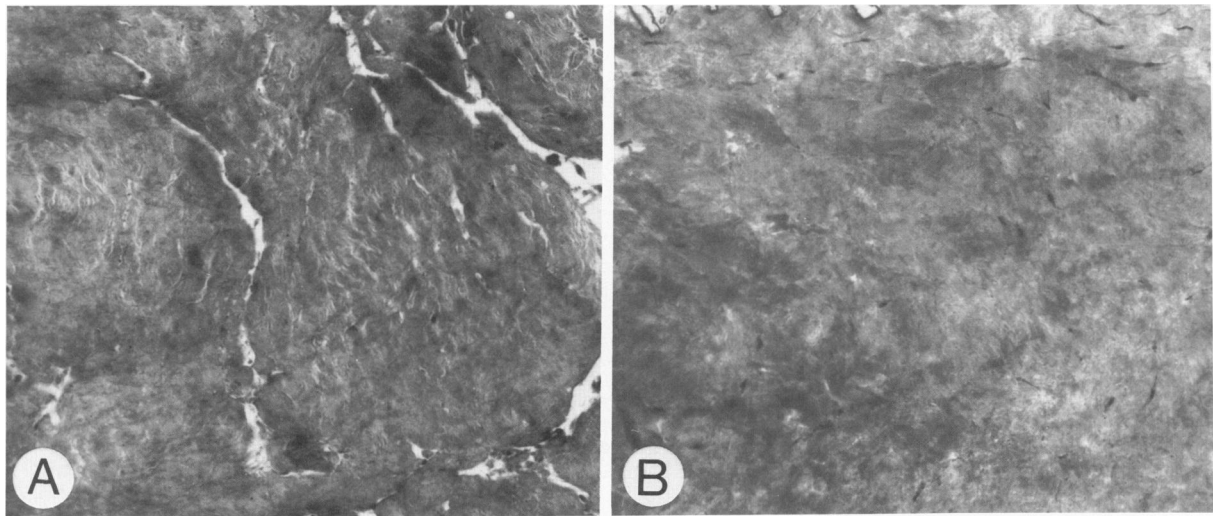


Figure 2—Light micrographs of sagittal sections of vehicle-containing chambers. (H&E, $\times 36$) **A**—Vehicle in collagen matrix. **B**—Vehicle in collagen/heparin 1.

Response to Single Growth Factors

PDGF

The addition of partially purified and purified PDGF to the chambers resulted in a consistent increase in cells relative to vehicle controls. The DNA content of PDGF/collagen-filled chambers was 1.5–2 times vehicle, and that of PDGF/CH1-filled chambers was 3–3.5 times vehicle (Figure 3). Thus, the addition of heparin to the collagen matrix significantly enhanced the response to PDGF. As shown in Figure 4A, incorporation of PDGF in a collagen matrix increased the cells in the lumen of each chamber relative to vehicle controls. In the CH1 matrix, this

increase was even more dramatic (Figure 4C). Higher magnifications of each section are presented in Figures 4B and 4D. The histologic appearance of the 10-day chambers containing PDGF resembled granulation tissue. Fibroblasts predominated, together with numerous macrophages, capillaries, and variable numbers of mononuclear cells (Figure 4B and D). Neutrophils were rare except in the lumen of the capillaries.

TGF β

Addition of TGF β to the collagen matrix resulted in significant increases in DNA content (Figure 3) and cell ingrowth when compared with vehicle. Use of the

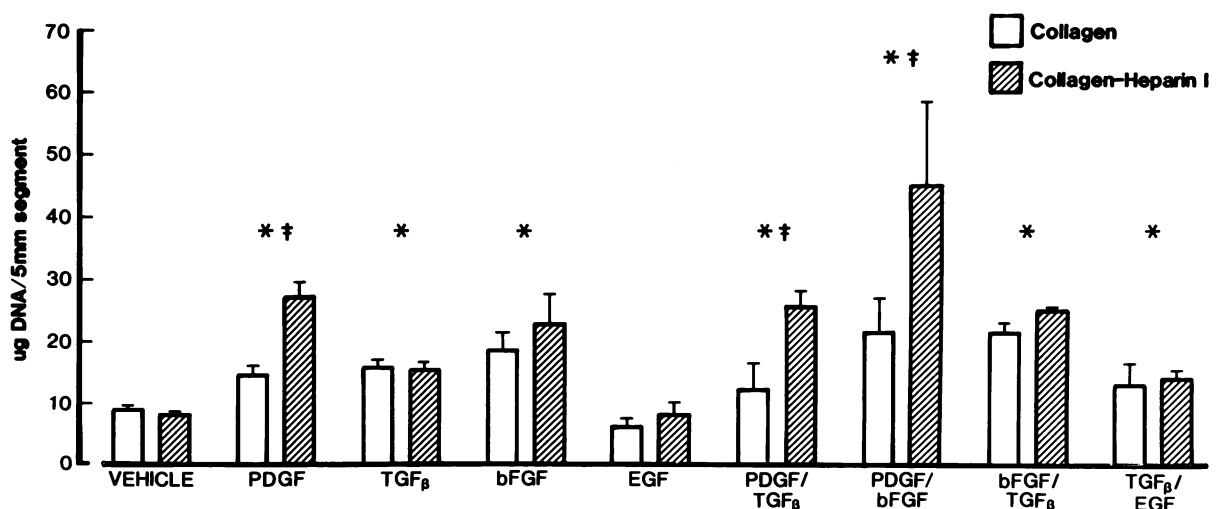


Figure 3—DNA content of chambers 10 days after insertion. Doses of growth factors were as follows: PDGF, 8 μ g/ml; TGF β , 4 μ g/ml; bFGF, 2 μ g/ml; EGF, 8 μ g/ml. $n = 12$ –25 for vehicle and single growth factors. For combinations or EGF alone, $n = 6$. *Significantly different from vehicle in appropriate collagen matrix (Kruskal-Wallis one-way ANOVA, Dunn's procedure, $P < 0.05$). †Significant difference between collagen formulations for indicated growth factor or combination (Mann-Whitney U test, $P < 0.05$). Bars represent mean \pm SEM.

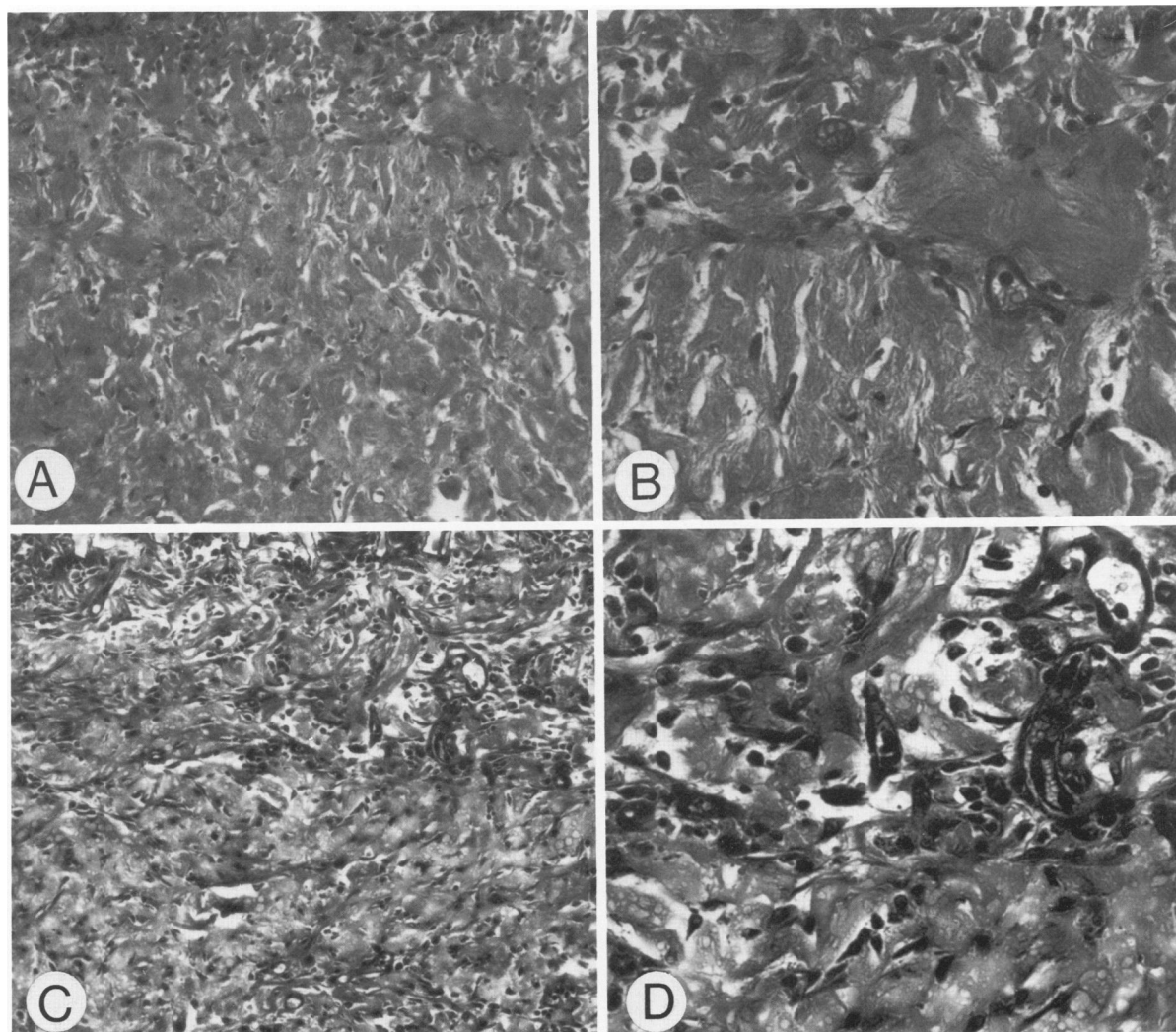


Figure 4—Light micrographs of sagittal sections of subcutaneous chambers. **A**—PDGF, 8 μ g/ml, in collagen. (H&E, $\times 36$) **B**—PDGF, 8 μ g/ml, in collagen. (H&E, $\times 91$) **C**—PDGF, 8 μ g/ml, in CH1. (H&E, $\times 36$) **D**—PDGF, 8 μ g/ml, in CH1. (H&E, $\times 91$)

collagen/heparin matrix did not enhance the response. Like PDGF and bFGF, TGF β resulted in a granulation tissue response in the subcutaneous chambers (Figure 5A and B). In contrast to the more uniform cell distribution seen with PDGF, fibroblasts, macrophages, and capillaries tended to be clustered in units.

FGF

The responses to bFGF were more variable than those seen with the other growth factors tested. In each collagen formulation, DNA contents ranged from as low as vehicle chambers to four to seven times greater than the vehicle (Figure 3). On average, bFGF in either collagen or CH1 caused a greater cellular response than vehicle. The histologic pattern was correspondingly variable. The collagen matrix in the

chambers ranged from relatively acellular to densely cellular and extremely vascularized tissue (Figure 5C and D). The capillaries were larger, dilated, and more prominent in the bFGF-containing chambers than in the PDGF- or TGF β chambers. Regions of leukocytic infiltration were common, a response not observed with any of the other growth factors. Areas of collagen reorganization (a decrease in density of the collagen matrix reflecting resorption of bovine collagen and secretion of new collagen by the cells) were more common in bFGF-filled chambers than in those filled with PDGF or TGF β .

A separate series of experiments was performed in an attempt to understand and control the variability of the bFGF responses. Every rat received four implanted chambers, each containing the same treatment. Chambers used for these rats were filled from a

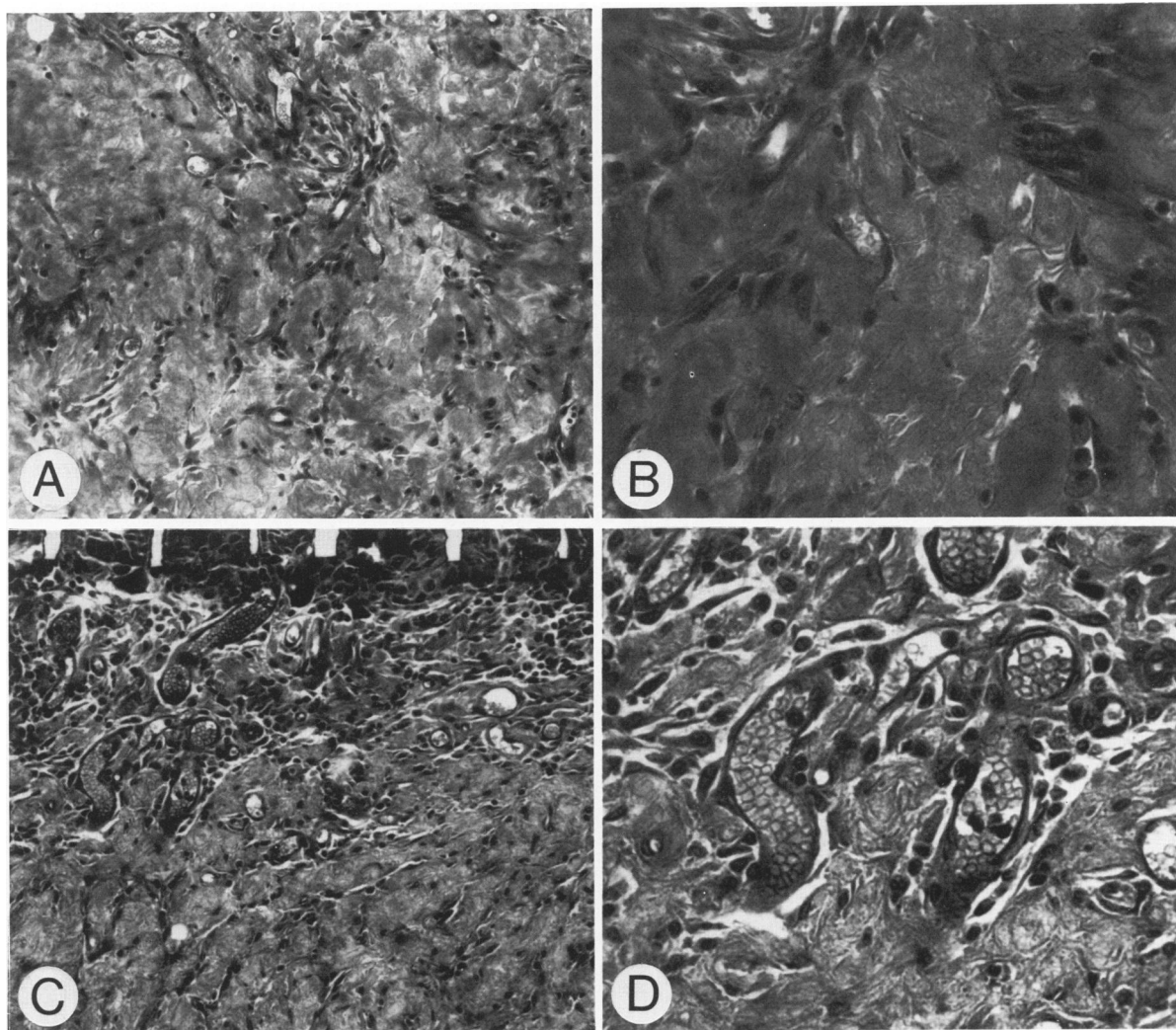


Figure 5—Light micrographs of sagittal sections of subcutaneous chambers. **A**—TGF β , 4 μ g/ml, in collagen. (H&E, $\times 36$) **B**—TGF β , 4 μ g/ml, in collagen. (H&E, $\times 91$) **C**—bFGF, 2 μ g/ml, in collagen. (H&E, $\times 36$) **D**—bFGF, 2 μ g/ml, in collagen. (H&E, $\times 91$)

single emulsified batch. This design allowed us to evaluate the variability in response in a given animal (ie, due to the position of the implant, lateral or medial) and the variability between animals. Additionally, a third collagen matrix was introduced into the design. In the CH1 matrix, most of the heparin was in solution and diffused rapidly out of the material when implanted.³⁰ The matrix designated CH2 was designed to minimize the free heparin so that most of the heparin in the material would be bound to the collagen fibrils. The rationale was that because bFGF binds to heparin, “immobilizing” (in relative terms) the heparin in the collagen matrix might help retain the bFGF, prolonging its residence in the chambers and potentially enhancing the responses or reducing the variability previously observed. The DNA con-

tents of the chambers from these experiments are summarized in Table 1. In contrast to earlier experiments, bFGF did not enhance the responses in collagen alone when compared with vehicle. Addition of either concentration of heparin to the matrix enhanced the response. The use of a lower heparin concentration (CH2) reduced the variability somewhat but did not eliminate it. The DNA content varied by as much as twofold between chambers that were inserted in the same rats, but no specific implant position could be correlated with consistent “high” or “low” responses. It is possible that the variability of the bFGF responses observed is related to the time point studied. bFGF responses might peak earlier than 10 days and thus exhibit a wider range of responses than PDGF and TGF β .

Table 1—Comparison of Responses to bFGF in Different Collagen Matrices*

Treatment	Collagen matrix	DNA content (μ /5 mm segment)	n
Vehicle	Collagen, CH1, CH2	10.8 (7.1–13.7)	20
2 μ g/ml bFGF	Collagen	11.2 (8.2–19.6)	24
2 μ g/ml bFGF	CH1	15.0 (5.0–36.6) ^{†‡}	24
2 μ g/ml bFGF	CH2	19.0 (9.9–35.0) ^{†‡§}	23

*Chambers were prepared as described in "Methods," inserted subcutaneously and left for 10 days. Collagen = 25 mg/ml bovine collagen, CH1 = collagen plus 250 μ g/ml heparin, CH2 = collagen plus 40 μ g/ml heparin. DNA values are reported as median (range).

[†]Significant difference from vehicle treatment (Kruskal–Wallis one-way ANOVA, $P < 0.05$; multiple comparisons: Dunn's procedure, experimentwise, $P < 0.10$).

[‡]Significant difference from bFGF in collagen (Kruskal–Wallis one-way ANOVA, $P < 0.05$; multiple comparisons: Dunn's procedure, experimentwise, $P < 0.10$).

[§]Significant difference from bFGF in CH1 (Kruskal–Wallis one-way ANOVA, $P < 0.05$; multiple comparisons: Dunn's procedure, experimentwise, $P < 0.10$).

EGF

EGF did not stimulate a response in this model at doses ranging from 100 to 800 ng/chamber. Neither DNA content nor histology was different from the vehicle controls at any of the doses tested. DNA content for EGF alone and combinations containing EGF at doses of 400 ng/chamber are shown in Figure 3. The EGF used in these experiments was active, as indicated by its ability to compete for binding to A431 cells with 125 I-EGF in a radioreceptor assay (data not shown).

Responses to Combinations of Growth Factors

It is unlikely that single growth factors are released from platelets or macrophages under physiologic conditions. In platelets, for example, PDGF, TGF β , and EGF seem to be stored in alpha granules^{8,17,24} and could potentially be released simultaneously in re-

sponse to the same stimulus. We therefore tested combinations of growth factors to determine whether their effects were additive, synergistic, or inhibitory. Chamber DNA contents in these experiments are summarized in Figure 3 to facilitate comparison of the effects of combinations with single growth factors. Each rat in these experiments had four chambers: vehicle, growth factor A, growth factor B, and a chamber containing both factors A and B. All chambers in a given rat had the same collagen matrix. In general, the combinations of two growth factors generated a response no different than either of the component factors alone. Figure 6A illustrates a typical response in a chamber filled with 8 μ g/ml partially purified PDGF and 2 μ g/ml bFGF. The combination of partially purified PDGF and bFGF showed a tendency toward synergy in individual chambers with the CH1 matrix, but the overall response was sufficiently variable that it can only be considered a trend. Histologically, the combinations reflected the characteris-

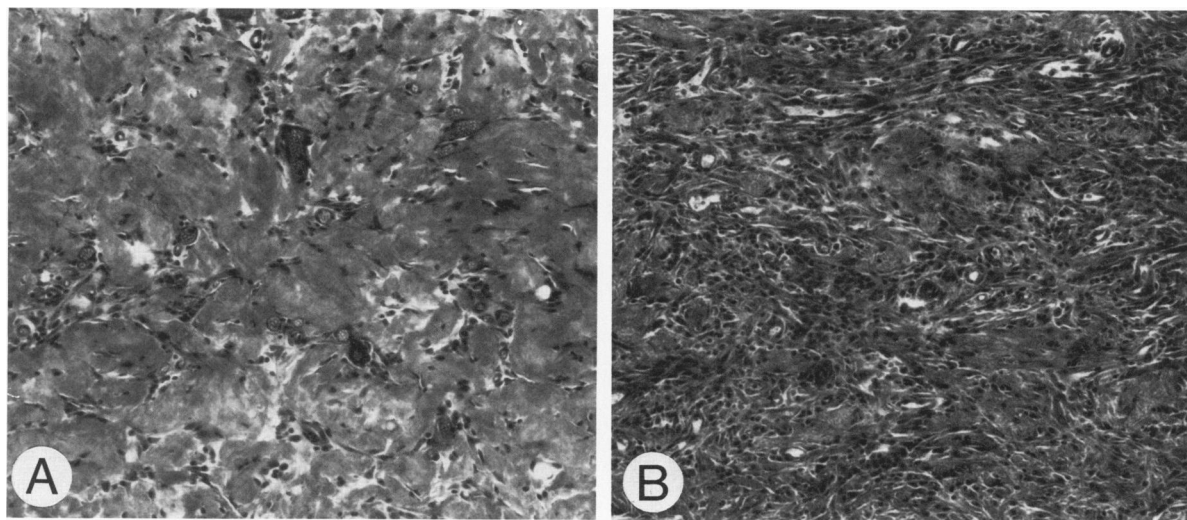


Figure 6—Light micrographs of sagittal sections of subcutaneous chambers containing combinations of growth factors. **A**—Partially purified PDGF, 8 μ g/ml, plus 4 μ g/ml TGF β in CH1. **B**—Partially purified PDGF, 8 μ g/ml, plus 2 μ g/ml bFGF in CH1. (H&E, $\times 36$)

tics of both factors involved. For example, the combination of PDGF and bFGF resulted in a greater fibroblast density than bFGF alone, and larger, more numerous capillaries than PDGF alone (Figure 6B).

Clearance of Growth Factors

Because two of the tested growth factors bind to heparin, we anticipated that incorporation of heparin might prolong growth factor retention in the collagen matrix and enhance the biologic response. PDGF and bFGF both bind to heparin and did produce enhanced responses in a collagen/heparin matrix when compared with a collagen matrix. For determining whether the enhanced biologic response could be attributed to longer retention of the factors in the chambers, and for obtaining kinetic information on the behavior of factors in the chambers, clearance studies were performed. Chambers were filled with an emulsion of growth factor, trace amounts of ^{125}I -labeled growth factor, and one of the collagen formulations; they were then implanted subcutaneously and removed at various times after insertion. Figures 7, 8, and 9 illustrate the results for PDGF, TGF β , and bFGF, respectively. The clearance of each factor occurred in two phases: an initial rapid clearance (presumably diffusion of free growth factor out of the chamber) and a second slower phase (perhaps reflecting the clearance of growth factor associated with the collagen matrix or PTFE of the chamber).

^{125}I -labeled PDGF was cleared rapidly from chambers filled with either collagen or CH1 (Figure 7). The relatively low “% counts remaining” at time

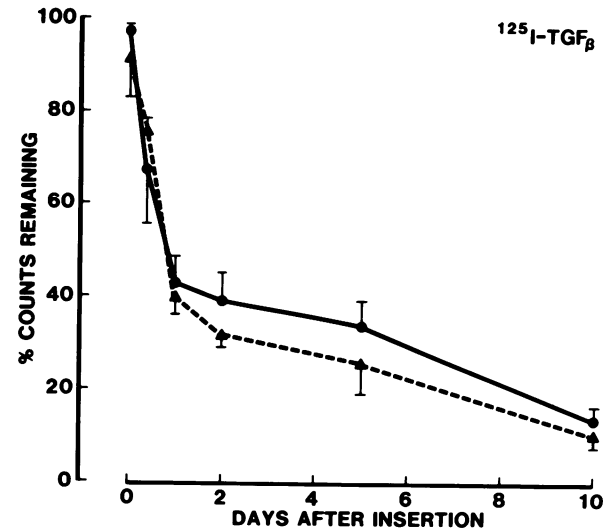


Figure 8—Clearance of ^{125}I -TGF β from subcutaneous chambers. $n = 4$ for each collagen formulation. ●, collagen; ▲, CH1. Points represent mean \pm SEM.

zero in the PDGF clearance are an artifact of the way the chambers were prepared. When we insert the chambers, some material exuded through the pores is lost in passing through the trocar. For the PDGF experiments, this meant that the counts determined before insertion were artificially high because some of those counts were lost in the insertion process. This problem was corrected in the TGF β and bFGF clearances by passing the chambers through a trocar before determining the precount. The half-life for the initial phase of PDGF clearance was 12 hours. The only difference between the amount of PDGF remaining

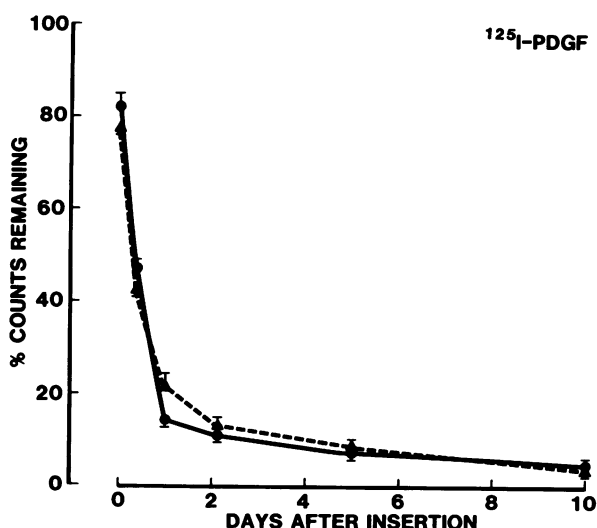


Figure 7—Clearance of ^{125}I -PDGF from subcutaneous chambers. $n = 6$ for each collagen formulation. ●, collagen; ▲, CH1. Points represent mean \pm SEM.

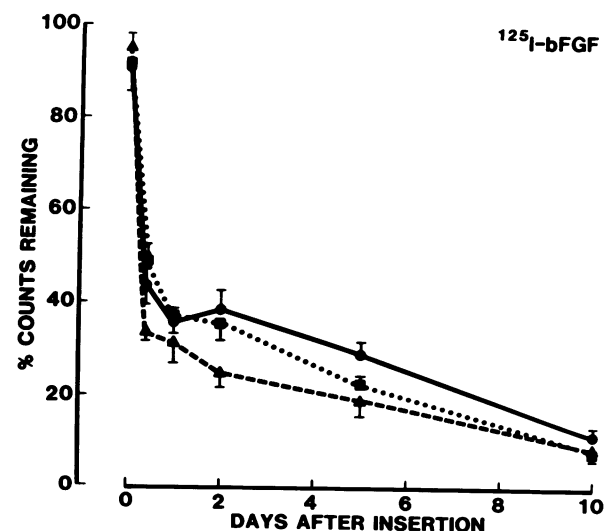


Figure 9—Clearance of ^{125}I -bFGF from subcutaneous chambers. $n = 4$ for collagen and CH2, $n = 3$ for CH1. ●, collagen; ▲, CH1; ■, CH2. Points represent mean \pm SEM.

in collagen versus CH1 occurred at 24 hours and was relatively small. It seems unlikely that such a small and transient difference in the PDGF remaining in the chambers could account for the dramatic increase in cell ingrowth observed. ^{125}I -labeled TGF β was cleared more slowly from the chambers than ^{125}I -labeled PDGF (Figure 8). The half-life for TGF β was 22 hours. There was no difference in the clearance from collagen or CH1-filled chambers. The clearance of bFGF was determined in all three collagen formulations. The initial clearance was rapid and quite similar from all three matrices, with a half-life of 9 hours (Figure 9). The slower phase appeared to occur at about the same rate from each matrix, but there tended to be less ^{125}I -bFGF left in the chambers filled with CH1 than with either collagen or CH2. This may reflect the amount of material free to diffuse out of the chambers in the first phase. It is possible that the bFGF mixed with CH1 became associated primarily with the heparin molecules in the suspension, most of which were free in solution³⁰ and could therefore readily diffuse out. In the collagen- or CH2-filled chambers, more of the bFGF might have been associated with the collagen matrix itself, binding either directly to the collagen or to heparin bound to collagen, and thus became a part of the slower releasing pool. The differences in clearance between the collagen matrices are subtle and do not support the hypothesis that a slower clearance of bFGF in the presence of heparin is responsible for the enhanced cellular responses.

Discussion

Specific platelet- and macrophage-derived growth factors can stimulate cellular proliferation and migration *in vitro*, but their capacities to function *in vivo* are not yet defined. In this series of experiments, PDGF, bFGF, and TGF β all produced neovascularization and fibroplasia in the chambers; EGF did not. Addition of heparin to the collagen matrix enhances the responses of the heparin-binding growth factors PDGF and bFGF, but has no effect on the TGF β or EGF responses. The clearance of PDGF, bFGF, and TGF β from the chambers is fairly rapid and is not altered by the addition of heparin. We anticipated that the addition of heparin might slow the clearance of PDGF and bFGF, but no differences were observed. Combining growth factors in the same chamber does not appear to alter the responses. This may be a function of the doses used. For PDGF and bFGF, these doses did not induce the maximum possible response, because addition of heparin to the matrix resulted in increased cellularity. We may not have

observed the maximum possible response to TGF β because the chambers could clearly accumulate more cells with PDGF or bFGF (compare Figures 5A and 6B). Thus, combinations of growth factors might reasonably be expected to show an additive effect. That they did not suggests that the extent of the response is limited by conditions other than the concentration of growth factor. At subthreshold doses, the growth factors might exhibit additivity or synergy. This possibility was not tested in these experiments.

Because heparin did not affect the retention of growth factors in the chambers, we considered other mechanisms by which it could enhance the cellular responses to PDGF and bFGF: alteration of the collagen fibrillar structure, direct effects of heparin on the target cells, potentiation of growth factor effects by heparin, and heparin effects on extracellular matrix modulation of cell growth. Addition of heparin to the soluble collagen preparations does have an effect on the characteristics of the matrix formed at 37 C. In the presence of heparin, the collagen fibrils are longer and form a more open lattice.^{30,32} The more open meshwork may facilitate cell ingrowth, but is not sufficient to account for our observations, because all chambers filled with collagen/heparin matrix did not show enhanced responses, compared with the same growth factor in collagen alone. Chambers containing vehicle in the collagen/heparin matrix were comparable to chambers containing vehicle in collagen.

The second possibility, that heparin may have direct effects, can be ruled out by similar arguments. If heparin had an effect, for example, on directed migration of fibroblasts or endothelial cells into the chambers, we would have expected to see an enhanced cellular response in all of the chambers containing collagen/heparin. This was not observed.

The third possibility, that heparin potentiates the activity of the growth factors *in vivo*, cannot be ruled out. Some precedent for such a function exists. Heparin stabilizes and potentiates the mitogenic and chemotactic activity of the acidic form of FGF for endothelial cells^{33,34} and protects both acidic and basic forms from heat or acid inactivation.³⁵ Additionally, heparin has been shown to potentiate the secretion of plasminogen activator from endothelial cells and the migration of endothelial cells in response to a crude 3T3-adipocyte secretion product.³⁶

A fourth possibility is that heparin may alter extracellular matrix effects on cell growth. Human skin fibroblasts grown on fibrillar collagen proliferate less in response to PDGF than do the same cells grown on bare tissue culture plastic, and heparin may modify this response (J. McPherson, unpublished observations).

The responses observed at 10 days in these studies might reflect a secondary stimulus, rather than a direct effect of the growth factor originally present in the chambers. Two observations support this argument. First, three of the growth factors used produced similar cellular responses in the chambers at 10 days despite different patterns of cellular response *in vitro*. Table 2 summarizes the *in vitro* actions of each of the growth factors examined which may be relevant to wound repair. Each growth factor has a different constellation of activities and target cells that could result in protease secretion, cell migration, cell proliferation, and secretion of extracellular matrix components in the chambers. Of necessity, Table 2 is a simplification. Effects reported on cultured cells for different growth factors were not determined for each growth factor in cells from the same tissue or species. The *in vivo* responses to growth factors observed in these studies do not necessarily correlate with their *in vitro* actions. For example, chambers treated with PDGF in a collagen/heparin matrix showed extensive neovascularization. This response would not be expected to be a direct effect of PDGF, because cultured endothelial cells have no receptors for PDGF⁴¹ and respond neither chemotactically nor mitogenically to PDGF in tissue culture. Second, the rapid initial clearance of each growth factor, particularly when compared with the pattern of cell ingrowth, suggests a secondary stimulus may be responsible for the responses observed at 10 days. Preliminary observations obtained at early time periods suggest that a classical pattern of inflammatory response occurs in these chambers. Two days after insertion, the predominant cell present is the polymorphonuclear leukocyte. By 5 days, the cell population has shifted and

consists primarily of monocytes and fibroblasts. Capillary appearance and extensive fibroblast proliferation does not occur until 8–10 days after the chambers are inserted, a time when 80–95% of the growth factor is gone from the chambers.

These observations support the hypothesis shown in Figure 10. Cells may enter the subcutaneous chamber either in response to a chemotactic stimulus by the specific growth factor in the chamber or as a part of a foreign-body response to the PTFE material of which the chamber is composed, or both. Once in the chamber, the granulocytes, monocytes, and lymphocytes thus attracted could produce chemotactic and mitogenic factors that would then be responsible for the influx of fibroblasts, capillaries, and white blood cells observed in the chambers at 10 days. PDGF, bFGF, or TGF β in the chambers might also modulate production or activation of factors secreted by these cells. This type of mechanism could account

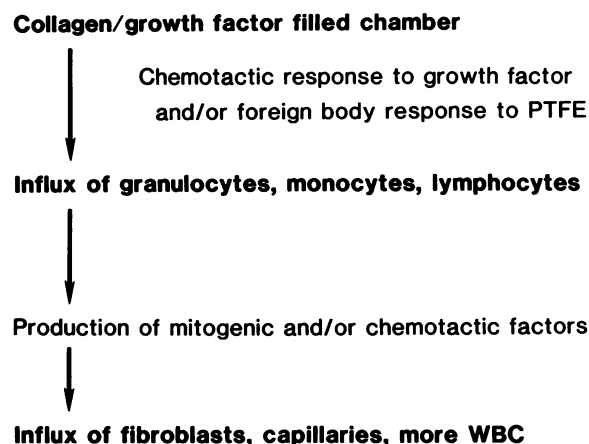


Figure 10—Hypothetical mechanism for growth factor actions in this model.

Table 2—In Vitro Actions of Selected Growth Factors*

Action	Cell†	Growth factor			
		PDGF	TGF β	bFGF	EGF
Chemotaxis	Endos	No effect ³⁷	?	Stimulates ^{‡34}	Stimulates§
	Fibs	Stimulates ³⁸	Stimulates ²²	Stimulates ^{‡51}	No effect ³⁸
	Monos	Stimulates ³⁹	Stimulates ²¹	?	?
Mitogenesis	Endos	No effect ^{40,41}	Inhibits ⁴⁷	Stimulates ^{14,52}	Stimulates ⁵⁵
	Fibs	Stimulates ⁴²	Stimulates ¹⁹ Inhibits ²⁰	Stimulates ⁵³	Stimulates ²⁷
Collagen synthesis	Fibs	Stimulates ⁴³	Stimulates ^{23,48}	?	?
		No effect ²³			
Collagenase secretion	Fibs	Stimulates ^{44,45}	Stimulates ⁴⁴	Stimulates ⁵⁰	Stimulates ^{44,50}
Plasminogen activator activity	Endos	?	?	Stimulates ⁵⁴	?
	Fibs	No effect ⁴⁶	Stimulates ⁴⁶ Decreases ⁴⁹	?	Stimulates ⁴⁹
Proteinase inhibitor secretion	Fibs	?	Stimulates ^{48,50}	Stimulates ⁵⁰	Stimulates ⁵⁰

*Superscript numbers refer to references cited.

†Endos, endothelial cells; Fibs, fibroblasts; Monos, monocyte/macrophages; ?, not known/reported.

‡Reported only for acidic FGF.

§Personal communication, Gary R. Grotendorst.

for the similarity of granulation tissue response to growth factors having very different *in vitro* patterns of activity.

Other investigators have also studied the effects of various growth factors in a variety of wound or wound-related models. Preparations of thrombin-stimulated platelet releasates, when incorporated in a collagen salve, have been shown to dramatically speed the healing of chronic nonhealing wounds.⁵⁶ In rats with suppressed wound healing responses, purified PDGF restored normal responses in wire mesh wound chambers, but had minimal effects in normal animals.^{57,58} In these experiments, PDGF increased the rate of collagen and cell accumulation in the chambers but did not change the magnitude of the response. Cartilage-derived growth factor (probably a bFGF-type molecule⁵⁹) produced a response similar to that we have observed with bFGF, albeit more rapid. Sponges injected with 500 ng of the cartilage-derived growth factor developed significant fibroplasia and neovascularization in 48–72 hours.⁶⁰ In a different model, eye-derived growth factor (also likely an FGF⁶¹) was shown to enhance the reepithelialization of burn blisters on swine epidermis.⁶² TGF β is also active in a wound healing model.⁶³ Wire mesh wound chambers were implanted subcutaneously in rats and repeatedly injected with crude TGF β . An increase in the DNA, collagen, and protein content of the chambers was observed after 9 days. These experiments were repeated and extended with pure TGF β by Lawrence and colleagues,⁵⁸ who showed that TGF β caused an increase in cellularity, protein, and DNA content of wire mesh chambers in normal and adriamycin-treated rats. Also, direct injection of TGF β subcutaneously in neonatal mice resulted in a profound fibroplasia and neovascularization.²³

Unlike the other growth factors tested, EGF appears to stimulate wound healing only in wound models that involve epithelial repair; in general, higher doses and multiple applications of EGF are required to generate a response. Topical application of EGF to full-thickness skin wounds in mice increased the rate of skin closure.⁶⁴ EGF has also been shown to increase collagen synthesis in cotton-pellet-induced granulomas.⁶⁵ Incorporation of EGF in a slow-release polymer, which was then implanted subcutaneously in a sponge, increased the accumulation of DNA, protein, and cells in the sponge in the short term but did not increase the maximal response achieved.⁶⁶ Collectively these data, in conjunction with the experiments presented in this paper, suggest that therapeutic applications of growth factors may be useful in wound repair once optimal combinations, doses, and delivery modes have been characterized.

The collagen-filled, subcutaneously implanted chamber described here provides a model for the study of the mechanisms of growth factor action *in vivo*. These initial observations demonstrate that growth factors can clearly modulate cell ingrowth but suggest that the mechanisms involved are more complex than previously thought. Elucidation of the cellular events, interactions, and responses by which each growth factor contributes to the formation of granulation tissue *in vivo* may ultimately help in the design of optimal growth factor combinations for specific wound healing applications.

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